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(74) Agents: WININGER, Aaron et al.; Squire, Sanders & Dempsey L.L.P., 600 Hansen Way, Palo Alto, CA 94304-1043 (US).

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(71) Applicant (for all designated States except US): ADVANCED CARDIOVASCULAR SYSTEMS, INC. [US/US]; 3200 Lakeside Drive, Santa Clara, CA 95054 (US).

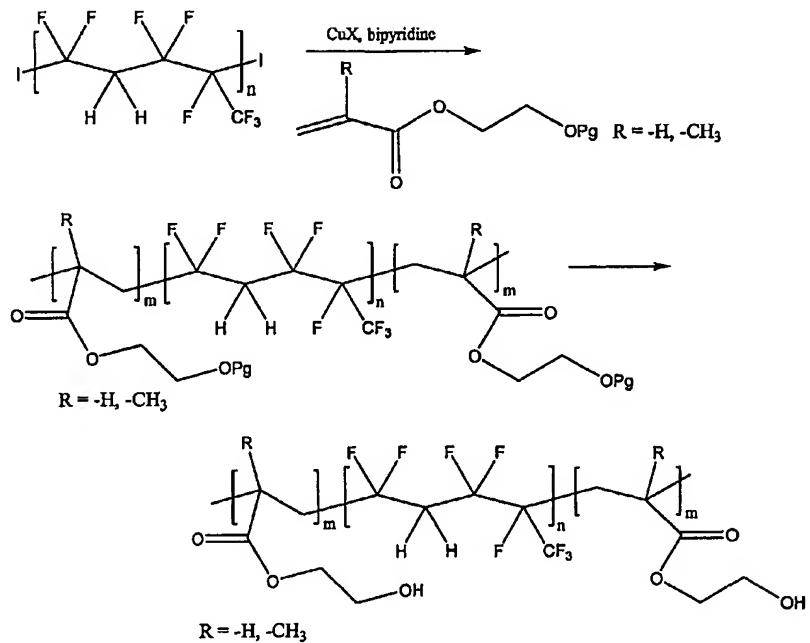
(72) Inventor; and

(75) Inventor/Applicant (for US only): CLAUDE, Charles, D. [US/US]; 1277 Poplar Avenue, Sunnyvale, CA 94086 (US).

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(54) Title: BLOCK COPOLYMERS OF ACRYLATES AND METHACRYLATES WITH FLUOROALKENES



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(57) Abstract: A block copolymer comprising a fluorinated block and a non-fluorinated block and method of making the block copolymer are provided. Also provided herein are a coating on an implantable device comprising the block copolymer and method of using the implantable device.



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BLOCK COPOLYMERS OF ACRYLATES AND METHACRYLATES WITH
FLUOROALKENES

BACKGROUND OF THE INVENTION

5 Field of the Invention

This invention generally relates to fluorinated and nonfluorinated block copolymer and composition formed therefrom useful for coating an implantable device such as a drug eluting stent.

Description of the Background

10 Blood vessel occlusions are commonly treated by mechanically enhancing blood flow in the affected vessels, such as by employing a stent. Stents are used not only for mechanical intervention but also as vehicles for providing biological therapy. To effect a controlled delivery of an active agent in stent medication, the stent can be coated with a biocompatible polymeric coating. The biocompatible polymeric coating can function either as a permeable layer or a
15 carrier to allow a controlled delivery of the agent.

Fluorinated polymers, such as poly(vinylidene fluoride-co-hexafluoropropylene), have been used to form drug-eluting stent (DES) coatings and can effectively control the release of pharmaceutical agents from a stent. DES coatings formed of these fluorinated polymers also have excellent mechanical properties and are biocompatible and biologically inert. However, polymers
20 of fluorinated olefins are very hydrophobic and may have low glass transition temperatures. Too high a hydrophobicity of the polymeric coating on a DES often reduces the permeability of the coating and thus slows down the release rate of a drug on the coating to an undesirable level.

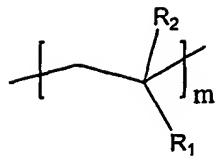
The polymer and methods of making the polymer disclosed herein address the above described problems.

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SUMMARY OF THE INVENTION

Disclosed herein is a fluorinated block copolymer comprising a fluorinated block and a non-fluorinated block. The non-fluorinated block of the polymer provides improved vascular responses and/or improved permeability for controlled release of pharmaceutical agents.

30 In accordance with one aspect of the invention, the non-fluorinated block comprises a polyolefinic block of the following structure:

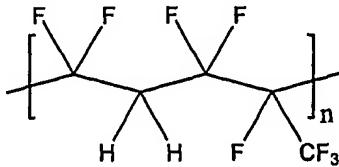


wherein R₁ is -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, naphthyl, -COOR₃, or -CONR₃R₄;

5 wherein R₂ is -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, or naphthalenyl; and

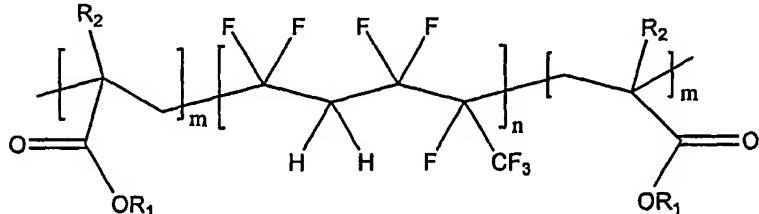
wherein R₃ and R₄ are -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, or -PEG.

In another embodiment, the fluorinated block can be, for example, a block of poly(fluorinated olefins), for example, a block having the following structure:



10

In a further embodiment, the fluorinated block copolymer has a structure of the following:



wherein R₁ is -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, or -PEG; and

15 wherein R₂ is -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, or naphthyl;.

The polymer can form a coating composition for coating an implantable device and/or a coating formed thereof for controlling the release rate of a bioactive agent. The block copolymer can be formed by polymerizing a non-fluorinated olefin such as acrylate, methacrylate, or styrene 20 in the presence of a copper catalyst, such as an ATRP (atom transfer radical polymerization) catalyst (see, for example, Matyjaszewski, K. *Controlled Radical Polymerization*; American Chemical Society: Washington, D.C., 1998; Vol. 685; Honigfort, M. E.; Brittain, W. J.; Bosanac, T.; Wilcox, C. S. *Polym. Prepr.* 2002, 43, 561), and a fluorinated di-halo macromer.

The fluorinated block copolymer can be used to form a coating composition comprising the fluorinated block copolymer alone or in combination with another material or polymer, optionally with a bioactive agent. The coating composition thus formed can be coated onto an implantable device such as a DES. The release rate of the bioactive agent on the DES can be
5 controlled by fine-tuning the hydrophobicity of the fluorinated block copolymer using a hydrophilic group such as ethylene glycol or polyethylene glycol.

BRIEF DESCRIPTION OF THE FIGURE

Figure 1 is a scheme for making a block copolymer having non-fluorinated blocks bearing a
10 hydrophilic ethylene glycol pendent groups.

DETAILED DESCRIPTION

A block copolymer comprising a fluorinated block and a non-fluorinated block and method of making the block copolymer are provided. Also provided herein are a coating on an
15 implantable device comprising the block copolymer and optionally a bioactive agent and method of using the implantable device.

Fluorinated Block Copolymer

A block of non-fluorinated polymer can be incorporated into a fluorinated polyolefin to form a block copolymer comprising a non-fluorinated block and a fluorinated block. The non-
20 fluorinated block provides the polymer with improved vascular responses and/or improved permeability which are desirable for controlled release of a bioactive agent.

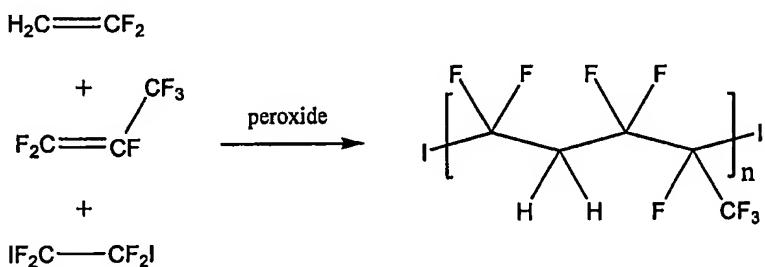
Fluorinated Blocks

In accordance with one aspect of the invention, the fluorinated block copolymer can be synthesized via a fluorinated macromer where at least one of the two termini of the macromer is
25 functionalized. In one embodiment, the termini of the fluorinated macromer are functionalized with two halo groups which can be two of chloro, bromo, iodo or a combination thereof. For example, the two halo groups can be two iodo groups. The functionalized fluorinated macromer can be then be used as a macro-initiator to form a block copolymer with non-fluorinated monomers. The term fluorinated macromer refers to a poly(fluoroolefin). As used herein, the
30 term poly(fluoroolefin) is used inter-exchangeably with the term poly(fluoroalkene).

In an embodiment, the dihalogen fluorinated macromer can be a poly(fluorinated olefin) bearing two halogen groups at both termini. This dihalo fluorinated macromer can be readily synthesized by polymerizing a fluorinated olefin or a mixture of a fluorinated olefin in the

presence of a dihalide and a peroxide (Ying, et al., *Polym. Preprints* 39(2):843 (1998); Zhang, et al., *Polymer* 40:1341 (1999); and Modena, et al., *J. fluorine Chem.* 4315(1989)). For example, a diiodo fluorinated macromer having as repeating unit $-\text{CF}_2\text{CH}_2\text{CF}_2\text{CF}(\text{CF}_3)-$ can be readily synthesized by polymerizing a mixture of vinylidene fluoride and 1,1,2,3,3,3-hexafluoropropene 5 in the presence of a peroxide and 1,2-diiodo-1,1,2,2-tetrafluoroethane (Scheme 1) (Ying, et al., *Polym. Preprints* 39(2):843 (1998); Zhang, et al., *Polymer* 40:1341 (1999); and Modena, et al., *J. fluorine Chem.* 43 15 (1989)).

Scheme 1

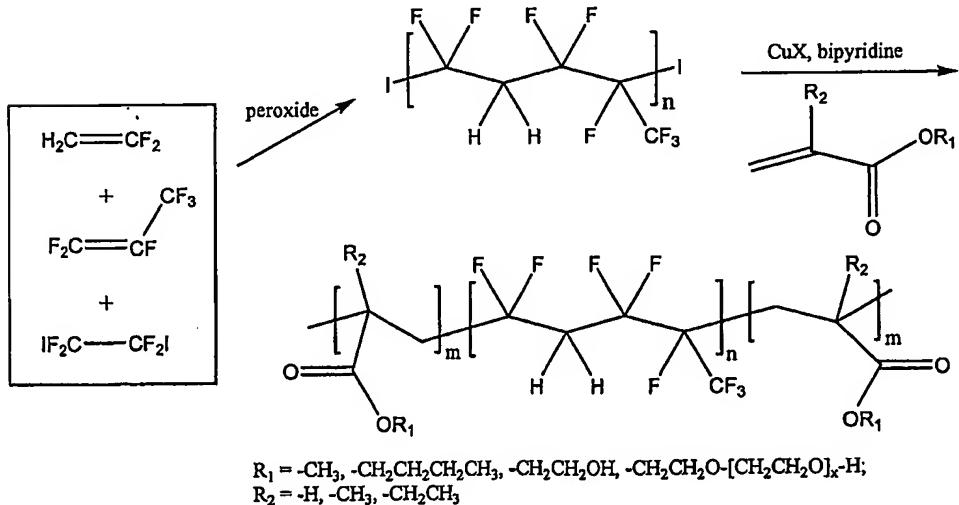
*Non-fluorinated Blocks*

Materials or polymers useful as the non-fluorinated blocks described herein include any polymers or macromers that can be directly attached to a fluorinated macromer described herein or polymers or macromers that can be functionalized to attach one or more functional groups such as hydroxyl, amino, halo, and carboxyl and other linking groups. Exemplary materials or polymers useful as the non-fluorinated blocks include, but are not limited to, polyolefins, 10 polyalkylene oxides, polyglycols such as poly(ethylene glycol) and poly(propylene glycol), polylactic acid, poly(lactide-co-glycolide), polyhydroxyalkanoate, poly(hydroxybutyrate-co-valerate); polyorthoester; polyanhydride; poly(glycolic acid-co-trimethylene carbonate); polyphosphoester; polyphosphoester urethane; poly(amino acids); poly(cyanoacrylates); poly(trimethylene carbonate); poly(iminocarbonate); copoly(ether-esters) (e.g. PEO/PLA); 15 polyalkylene oxalates; polyphosphazenes; biomolecules, such as fibrin, fibrinogen, cellulose, starch, collagen and hyaluronic acid; polyurethanes; silicones; polyesters; polyolefins; polyisobutylene and ethylene-alphaolefin copolymers; acrylic polymers and copolymers; vinyl halide polymers and copolymers, such as polyvinyl chloride; polyvinyl ethers, such as polyvinyl methyl ether; polyvinylidene halides, such as polyvinylidene fluoride and polyvinylidene chloride; 20 polyacrylonitrile; polyvinyl ketones; polyvinyl aromatics, such as polystyrene; polyvinyl esters, such as polyvinyl acetate; copolymers of vinyl monomers with each other and olefins, such as ethylene-methyl methacrylate copolymers, acrylonitrile-styrene copolymers, ABS resins, and 25

ethylene-vinyl acetate copolymers; polyamides, such as Nylon 66 and polycaprolactam; alkyd resins; polycarbonates; polyoxymethylenes; polyimides; polyethers; epoxy resins; polyurethanes; rayon; rayon-triacetate; cellulose acetate; cellulose butyrate; cellulose acetate butyrate; cellophane; cellulose nitrate; cellulose propionate; cellulose ethers; and carboxymethyl cellulose. As used herein, the term "non-fluorinated block" may include fluorinated pendant groups such as -CF₃.

In another embodiment, the non-fluorinated block can be incorporated into the fluorinated block by polymerizing an unsaturated compound, for example, acrylate or methacrylate using a catalyst such as a copper catalyst in the presence of a di-halo fluorinated macromer. For example, a block copolymer with a perfluorinated block can be made from monomers including vinylidene 10 fluoride, hexafluoropropylene, tetrafluoroethylene, and other fluorinated olefins in the presence of a fluorinated dihalide under conditions of a standard radical polymerization (Ying et al., 1998; Zhang et al., 1999; and Modena et al., 1989, *supra*) to form a fluorinated di-halo macromer which can undergo polymerization with an unsaturated compound via an ATRP catalyst, as shown in Scheme 2 (Perrier, et al., *Tetrahedron Lett* 58 4053 (2002); Jo, et al., *Polym Bull (Berlin)* 44:1 15 (2002)).

Scheme 2

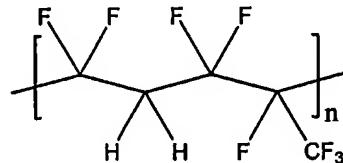


The fluorinated di-halo macromer can be used to attach the macromer to many other types of polymers. For example, the di-halo groups can be replaced by many functional groups, for example, functional groups bearing a negative or partially negative charge. This allows the formation of a block copolymer bearing a poly(fluorinated olefin) block and one or two blocks of other nature such as polyesters, polyethers, polyanhydrides, polyglycols, poly(alkylene oxides),

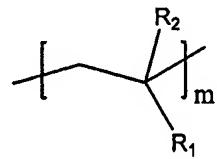
polyhydroxyalkanoates, polyphosphazenes, polyurethanes, or other biocompatible polymers commonly used in the art of drug delivery. The fluorinated di-halo macromer can form into a metalloc macromer, which may be useful for linking the macromer with another biocompatible block or polymer.

5 As shown in Scheme 2, many different polymers can be made. For example, in addition to variations of the substituents such as R₁ and R₂ in Scheme 2, the ratio of the fluorinated block to the non-fluorinated block can be varied, leading to formation of block copolymers having different level of hydrophobicity and permeability with different surface and mechanical properties. For example, following the method shown in Scheme 2, block copolymers comprising 10 a fluorinated block and non-fluorinated blocks of hydrophilic monomers such as hydroxyethyl methacrylate, hydroxypropyl methacrylate, N-vinyl pyrrolidone, or polyethylene glycol acrylate can be synthesized. The monomers with labile hydroxy functionalities can be protected with a protecting group (Pg), which can be cleaved upon completion of the reaction (Figure 1). The 15 protecting group can be, for example, t-butyl-dimethylsilane or trimethylsilane which can then be deprotected in stoichiometric yields with acidic hydrolysis.

In one embodiment, the block copolymer described herein has a fluorinated block having the following structure:



and a non-fluorinated block has the following structure:



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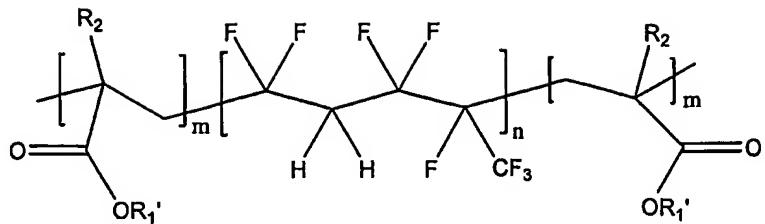
wherein R₁ can be -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, naphthyl, -COOR₃, or -CONR₃R₄;

wherein R₂ can be -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, or naphthalenyl; and

25

wherein R₃ and R₄ can be -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, or -PEG.

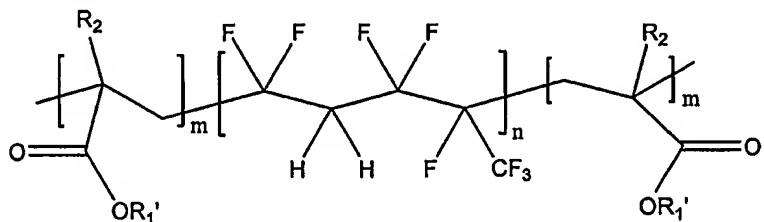
In another embodiment, the block copolymer has a formula of the following structure:



wherein R₁ can be -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, or -PEG, and

wherein R₂ can be -H or -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl or naphthyl.

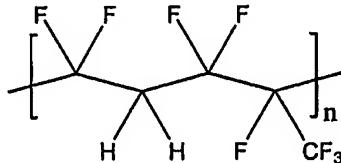
In a further embodiment, the block copolymer has a formula of the following structure:



wherein R₁ is -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, or -PEG, and

wherein R₂ is -H or -CH₃.

In still a further embodiment, the block copolymer described herein has a fluorinated block having the following structure:



and a non-fluorinated block that can be polyesters, polyethers, polyanhydrides, polyglycols, poly(alkylene oxides), polyhydroxyalkanoates, polyphosphazenes, polyurethanes, or a combination thereof.

Compositions of Fluorinated Block Copolymers

The Fluorinated block copolymer described above can be used to form coating compositions for coating an implantable device, for example, a stent. The fluorinated block copolymer can be used alone or in combination with another polymer. For use as DES coatings, the composition can include a bioactive agent.

Bioactive Agents

- The bioactive agent can be any agent that is biologically active, for example, a therapeutic, prophylactic, or diagnostic agent. Examples of suitable therapeutic and prophylactic agents 5 include synthetic inorganic and organic compounds, proteins and peptides, polysaccharides and other sugars, lipids, and DNA and RNA nucleic acid sequences having therapeutic, prophylactic or diagnostic activities. Nucleic acid sequences include genes, antisense molecules which bind to complementary DNA to inhibit transcription, and ribozymes. Compounds with a wide range of molecular weight can be encapsulated, for example, between 100 and 500,000 grams or more per 10 mole. Examples of suitable materials include proteins such as antibodies, receptor ligands, and enzymes, peptides such as adhesion peptides, saccharides and polysaccharides, synthetic organic or inorganic drugs, and nucleic acids. Examples of materials which can be encapsulated include enzymes, blood clotting factors, inhibitors or clot dissolving agents such as streptokinase and tissue plasminogen activator; antigens for immunization; hormones and growth factors; 15 polysaccharides such as heparin; oligonucleotides such as antisense oligonucleotides and ribozymes and retroviral vectors for use in gene therapy. Representative diagnostic agents are agents detectable by x-ray, fluorescence, magnetic resonance imaging, radioactivity, ultrasound, computer tomography (CT) and positron emission tomography (PET). Ultrasound diagnostic agents are typically a gas such as air, oxygen or perfluorocarbons.
- 20 In the case of controlled release, a wide range of different bioactive agents can be incorporated into a controlled release device. These include hydrophobic, hydrophilic, and high molecular weight macromolecules such as proteins. The bioactive compound can be incorporated into polymeric coating in a percent loading of between 0.01% and 70% by weight, more preferably between 1% and 35% by weight.
- 25 In one embodiment, the bioactive agent can be for inhibiting the activity of vascular smooth muscle cells. More specifically, the bioactive agent can be aimed at inhibiting abnormal or inappropriate migration and/or proliferation of smooth muscle cells for the inhibition of restenosis. The bioactive agent can also include any substance capable of exerting a therapeutic or prophylactic effect in the practice of the present invention. For example, the bioactive agent 30 can be for enhancing wound healing in a vascular site or improving the structural and elastic properties of the vascular site. Examples of active agents include antiproliferative substances such as actinomycin D, or derivatives and analogs thereof (manufactured by Sigma-Aldrich 1001 West Saint Paul Avenue, Milwaukee, WI 53233; or COSMEGEN available from Merck).

Synonyms of actinomycin D include dactinomycin, actinomycin IV, actinomycin I₁, actinomycin X₁, and actinomycin C₁. The bioactive agent can also fall under the genus of antineoplastic, anti-inflammatory, antiplatelet, anticoagulant, antifibrin, antithrombin, antimitotic, antibiotic, antiallergic and antioxidant substances. Examples of such antineoplastics and/or antimitotics 5 include paclitaxel (e.g. TAXOL[®] by Bristol-Myers Squibb Co., Stamford, Conn.), docetaxel (e.g. Taxotere[®], from Aventis S.A., Frankfurt, Germany) methotrexate, azathioprine, vincristine, vinblastine, fluorouracil, doxorubicin hydrochloride (e.g. Adriamycin[®] from Pharmacia & Upjohn, Peapack N.J.), and mitomycin (e.g. Mutamycin[®] from Bristol-Myers Squibb Co., Stamford, Conn.). Examples of such antiplatelets, anticoagulants, antifibrin, and antithrombins include 10 sodium heparin, low molecular weight heparins, heparinoids, hirudin, argatroban, forskolin, vapiprost, prostacyclin and prostacyclin analogues, dextran, D-phe-pro-arg-chloromethylketone (synthetic antithrombin), dipyridamole, glycoprotein IIb/IIIa platelet membrane receptor antagonist antibody, recombinant hirudin, and thrombin inhibitors such as Angiomax α (Biogen, Inc., Cambridge, Mass.). Examples of such cytostatic or antiproliferative agents include 15 angiopeptin, angiotensin converting enzyme inhibitors such as captopril (e.g. Capoten[®] and Capozide[®] from Bristol-Myers Squibb Co., Stamford, Conn.), cilazapril or lisinopril (e.g. Prinivil[®] and Prinzide[®] from Merck & Co., Inc., Whitehouse Station, NJ); calcium channel blockers (such as nifedipine), colchicine, fibroblast growth factor (FGF) antagonists, fish oil 20 (omega 3-fatty acid), histamine antagonists, lovastatin (an inhibitor of HMG-CoA reductase, a cholesterol lowering drug, brand name Mevacor[®] from Merck & Co., Inc., Whitehouse Station, NJ), monoclonal antibodies (such as those specific for Platelet-Derived Growth Factor (PDGF) receptors), nitroprusside, phosphodiesterase inhibitors, prostaglandin inhibitors, suramin, serotonin blockers, steroids, thioprotease inhibitors, triazolopyrimidine (a PDGF antagonist), and nitric oxide. An example of an antiallergic agent is permirolast potassium. Other therapeutic 25 substances or agents which may be appropriate include alpha-interferon, genetically engineered epithelial cells, tacrolimus, dexamethasone, and rapamycin and structural derivatives or functional analogs thereof, such as 40-O-(2-hydroxy)ethyl-rapamycin (known as Everolimus, available from Novartis as CerticanTM), 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin. The foregoing substances are listed by way of 30 example and are not meant to be limiting. Other active agents which are currently available or that may be developed in the future are equally applicable.

The dosage or concentration of the bioactive agent required to produce a favorable therapeutic effect should be less than the level at which the bioactive agent produces toxic effects

and greater than the level at which non-therapeutic results are obtained. The dosage or concentration of the bioactive agent required to inhibit the desired cellular activity of the vascular region can depend upon factors such as the particular circumstances of the patient; the nature of the trauma; the nature of the therapy desired; the time over which the ingredient administered 5 resides at the vascular site; and if other active agents are employed, the nature and type of the substance or combination of substances. Therapeutic effective dosages can be determined empirically, for example by infusing vessels from suitable animal model systems and using immunohistochemical, fluorescent or electron microscopy methods to detect the agent and its effects, or by conducting suitable in vitro studies. Standard pharmacological test procedures to 10 determine dosages are understood by one of ordinary skill in the art.

Methods of Using the Coating Composition

The coating composition can be coated onto any implantable device by any established coating process, e.g., a spray process. Generally, the coating process involves dissolving or 15 suspending the composition in a solvent to form a solution or a suspension of the coating composition, and then applying the solution or suspension to an implantable device such as a stent.

As used herein, an implantable device may be any suitable medical substrate that can be implanted in a human or veterinary patient. A exemplary implantable device is a stent such as 20 DES. Examples of stents include self-expandable stents, balloon-expandable stents, and stent-grafts. Other exemplary implantable devices include grafts (e.g., aortic grafts), artificial heart valves, cerebrospinal fluid shunts, pacemaker electrodes, and endocardial leads (e.g., FINELINE and ENDOTAK, available from Guidant Corporation, Santa Clara, CA). The underlying structure of the device can be of virtually any design. The device can be made of a metallic material or an 25 alloy such as, but not limited to, cobalt chromium alloy (ELGILOY), stainless steel (316L), high nitrogen stainless steel, e.g., BIODUR 108, cobalt chrome alloy L-605, "MP35N," "MP20N," ELASTINITE (Nitinol), tantalum, nickel-titanium alloy, platinum-iridium alloy, gold, magnesium, or combinations thereof. "MP35N" and "MP20N" are trade names for alloys of cobalt, nickel, chromium and molybdenum available from Standard Press Steel Co., Jenkintown, 30 PA. "MP35N" consists of 35% cobalt, 35% nickel, 20% chromium, and 10% molybdenum. "MP20N" consists of 50% cobalt, 20% nickel, 20% chromium, and 10% molybdenum. Devices made from bioabsorbable or biostable polymers could also be used with the embodiments of the present invention.

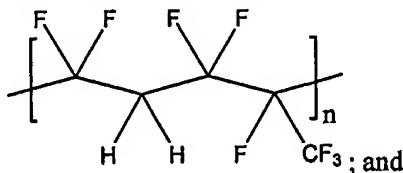
The implantable device described herein can be used to treat any medical condition, for example, a vascular disorder in an animal such as a human. Representative medical conditions that can be treated using the implantable device described herein include, but are not limited to, cancer, restenosis, vulnerable plaque, thrombosis or inflammation.

5 While particular embodiments of the present invention have been shown and described, it will be obvious to those skilled in the art that changes and modifications can be made without departing from this invention in its broader aspects. Therefore, the appended claims are to encompass within their scope all such changes and modifications as fall within the true spirit and scope of this invention.

CLAIMS

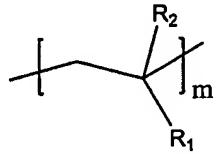
What is claimed is:

1. A block copolymer comprising a fluorinated block and at least one non-fluorinated block, wherein the fluorinated block has the following structure:



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wherein the non-fluorinated block has the following structure:

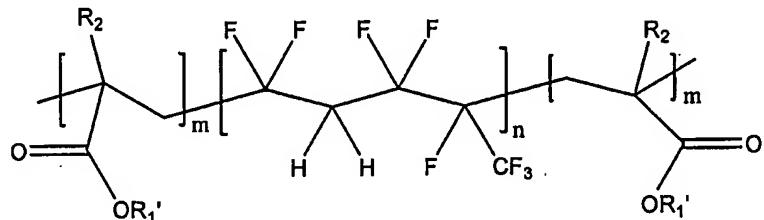


wherein R1 is selected from the group consisting of -CH3, -CF3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -phenyl, naphthyl, -COOR3, and -CONR3R4;

10 wherein R2 is selected from the group consisting of -H, -CH3, -CF3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -phenyl, and naphthalenyl; and

wherein R3 and R4 are selected from the group consisting of -CH3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -CH2CH2OH, and -PEG.

2. The block copolymer of claim 1 having a formula of the following structure:



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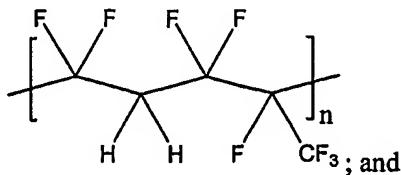
wherein R1 is selected from the group consisting of -CH3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -CH2CH2OH, and -PEG, and

wherein R2 is selected from the group consisting of -H or -CH3, -CF3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -phenyl and naphthyl.

20 3. The block copolymer of claim 2 wherein R1 is -CH3, -CH2CH3, -CH2CH2CH3, -CH2CH2CH2CH3, -CH2CH2OH, or -PEG, and

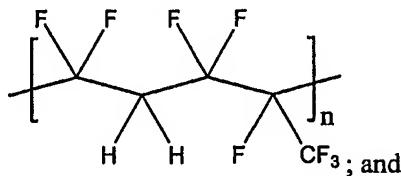
wherein R2 is -H or -CH3.

4. A block copolymer comprising a fluorinated block and at least one non-fluorinated block, wherein the fluorinated block has the following structure:



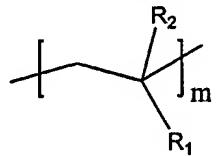
wherein the non-fluorinated block is a polymer selected from the group consisting of
 5 polyesters, polyethers, polyanhydrides, polyglycols, poly(alkylene oxides),
 polyhydroxyalkanoates, polyphosphazenes, polyurethanes, and a combination thereof.

5. A polymeric coating composition comprising a block copolymer which comprises a fluorinated block and at least one non-fluorinated block, wherein the fluorinated block has the following structure:



10

wherein the non-fluorinated block has the following structure:



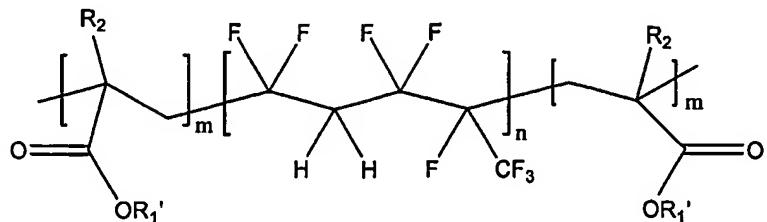
wherein R₁ is selected from the group consisting of -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, naphthyl, -COOR₃, and -CONR₃R₄;

15

wherein R₂ is selected from the group consisting of -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, and naphthalenyl; and

wherein R₃ and R₄ are selected from the group consisting of -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, and -PEG.

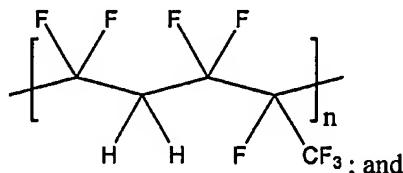
6. The coating composition of claim 5 wherein the block copolymer has a formula of the following structure:



wherein R_1' is selected from the group consisting of $-\text{CH}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{OH}$, and $-\text{PEG}$, and
 5 wherein R_2 is selected from the group consisting of $-\text{H}$ or $-\text{CH}_3$, $-\text{CF}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{phenyl}$ and naphthyl .

7. The coating composition of claim 6 wherein R_1' is selected from the group consisting of $-\text{CH}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{OH}$, or $-\text{PEG}$, and
 10 wherein R_2 is $-\text{H}$ or $-\text{CH}_3$.

8. A polymeric coating composition comprising a block copolymer which comprises a fluorinated block and at least one non-fluorinated block, wherein the fluorinated block has the following structure:



15 wherein the non-fluorinated block is a polymer selected from the group consisting of polyesters, polyethers, polyanhydrides, polyglycols, poly(alkylene oxides), polyhydroxyalkanoates, polyphosphazenes, polyurethanes, and a combination thereof.

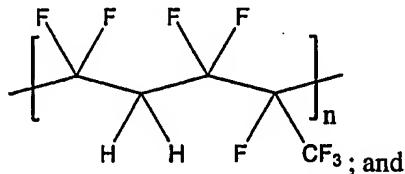
9. The coating composition of claim 5 further comprising a bioactive agent.
10. The coating composition of claim 6 further comprising a bioactive agent.
- 20 11. The coating composition of claim 7 further comprising a bioactive agent.
12. The coating composition of claim 8 further comprising a bioactive agent.
13. The coating composition of claim 9 wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

14. The coating composition of claim 10 wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

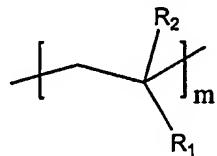
5 15. The coating composition of claim 11 wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

16. An implantable device comprising a coating which comprises a block copolymer, 10 the block copolymer comprising a fluorinated block and at least one non-fluorinated block.

17. The implantable device of claim 16, wherein the fluorinated block has the following structure:



wherein the non-fluorinated block has the following structure:



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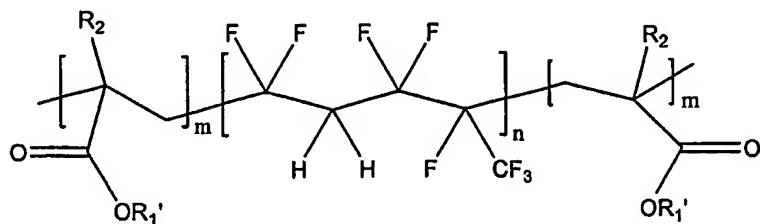
wherein R₁ is selected from the group consisting of -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, naphthyl, -COOR₃, and -CONR₃R₄;

wherein R₂ is selected from the group consisting of -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, and naphthalenyl; and

20

wherein R₃ and R₄ are selected from the group consisting of -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, and -PEG.

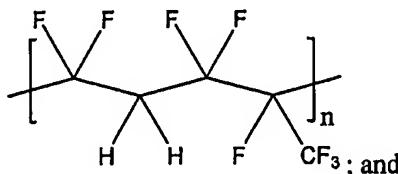
18. The implantable device of claim 17, wherein the block copolymer has a formula of the following structure:



wherein R_1' is selected from the group consisting of $-\text{CH}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{OH}$, and $-\text{PEG}$, and
5 wherein R_2 is selected from the group consisting of $-\text{H}$ or $-\text{CH}_3$, $-\text{CF}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{phenyl}$ and naphthyl .

19. The implantable device of claim 18 wherein R_1' is selected from the group consisting of $-\text{CH}_3$, $-\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{CH}_2\text{CH}_3$, $-\text{CH}_2\text{CH}_2\text{OH}$, or $-\text{PEG}$, and
10 wherein R_2 is $-\text{H}$ or $-\text{CH}_3$.

20. The implantable device of claim 16, wherein the fluorinated block has the following structure:



wherein the non-fluorinated block is a polymer selected from the group consisting of
15 polyesters, polyethers, polyanhydrides, polyglycols, poly(alkylene oxides),
polyhydroxyalkanoates, polyphosphazenes, polyurethanes, and a combination thereof.

21. The implantable device of claim 16, which is a drug-eluting stent, wherein the coating further comprises a bioactive agent.

22. The implantable device of claim 17, which is a drug-eluting stent, wherein the coating further comprises a bioactive agent.

23. The implantable device of claim 18, which is a drug-eluting stent, wherein the coating further comprises a bioactive agent.

24. The implantable device of claim 19, which is a drug-eluting stent, wherein the coating further comprises a bioactive agent.

25. The implantable device of claim 20, which is a drug-eluting stent, wherein the coating further comprises a bioactive agent.

26. The implantable device of claim 21, wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

5 27. The implantable device of claim 22, wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

10 28. The implantable device of claim 23, wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

15 29. The implantable device of claim 24, wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

20 30. The implantable device of claim 25, wherein the bioactive agent is selected from the group consisting of tacrolimus, dexamethasone, rapamycin, Everolimus, 40-O-(3-hydroxy)propyl-rapamycin, 40-O-[2-(2-hydroxy)ethoxy]ethyl-rapamycin, and 40-O-tetrazole-rapamycin.

31. A method of treating restenosis or vulnerable plaque, comprising implanting in a human being in need thereof the implantable device of claim 16.

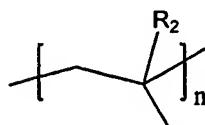
32. A method of treating restenosis or vulnerable plaque, comprising implanting in a human being in need thereof the implantable device of claim 17.

25 33. A method of treating restenosis or vulnerable plaque, comprising implanting in a human being in need thereof the implantable device of claim 26.

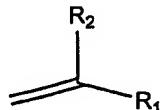
34. A method of treating restenosis or vulnerable plaque, comprising implanting in a human being in need thereof the implantable device of claim 27.

30 35. A method of treating restenosis or vulnerable plaque, comprising implanting in a human being in need thereof the implantable device of claim 28.

36. A method of synthesizing a block copolymer comprising a fluorinated block and at least a block of the following structure:



, comprising copolymerizing a monomer having the structure of



5 in the presence of a di-halo macromer,

wherein R₁ is selected from the group consisting of -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, naphthyl, -COOR₃, and -CONR₃R₄;

wherein R₂ is selected from the group consisting of -H, -CH₃, -CF₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -phenyl, and naphthalenyl; and

10 wherein R₃ and R₄ are selected from the group consisting of -CH₃, -CH₂CH₃, -CH₂CH₂CH₃, -CH₂CH₂CH₂CH₃, -CH₂CH₂OH, and -PEG, and

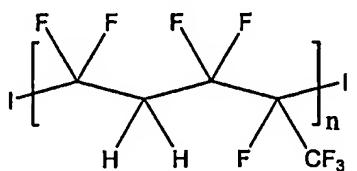
wherein the di-halo macromer is selected from the group consisting of di-chloro macromer, di-bromo macromer, di-iodo macromer and a combination thereof.

37. The method of claim 36 wherein the di-halo macromer is formed by polymerizing 15 a fluorinated olefin in the presence of a dihalide.

38. The method of claim 37 wherein the fluorinated olefin is selected from the group consisting of vinylidene fluoride, hexafluoropropylene, tetrafluoroethylene, and a combination thereof.

39. The method of claim 38 wherein the di-halo macromer is prepared by 20 polymerizing a mixture of vinylidene fluoride and 1,1,2,3,3-hexafluoropropylene in the presence of 1,2-diiodo-1,1,2,2-difluoroethylene.

40. The method of claim 39 the di-halo macromer has a structure of



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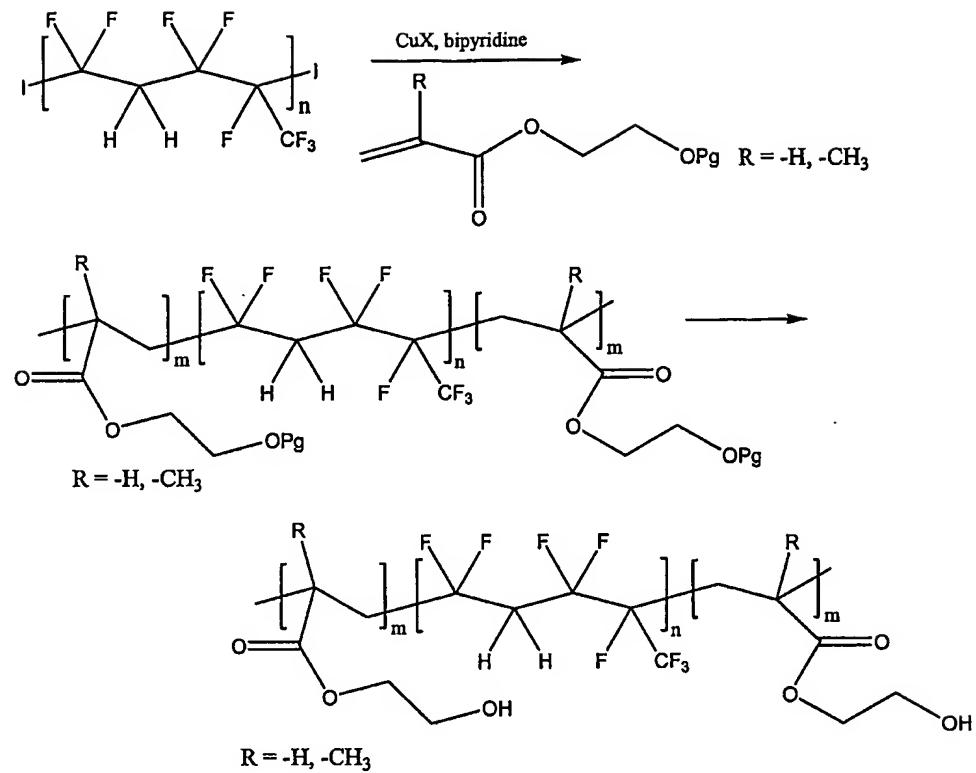


Figure 1